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Proceedings will be useful for students and researchers working in the following areas: pattern recognition and image analysis; knowledge processing and representation; knowledge based decision support system, fuzzy mathematics and systems, applications of pattern recognition and image analysis.

Papers are reviewed by at least two reviewers and approved by Program Committee. All papers have been photographically reproduced exactly as submitted by authors on their own responsibility.

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Section list

0	Plenary Papers	13
1	Pattern Recognition and Image Processing	25
2	Data Analysis	. 149
3	Signal Processing	. 219
4	Systems and Parallel Architectures for Signal and Image Processing	268
5	Knowledge-Based Expert and Decision Support Systems	. 303
6	Application of Pattern Recognition and Informaton Processing	351
7	3D Image Processing and Modeling	. 442

Contents

Committees PRIP'2011	9
Welcome from the Honorary Conference Chair and Co-Chairs	11
Key-note speakers	12
Plenary Papers	13
Robert E. Hiromoto GPU and Multi-cores: Computational Thinking – Art and Science	13
Chanin Joochim, Hubert Roth, Chayakorn Netramai Robust 3D Map Building Using 3D sensors	17
Janusz Zalewski Latest Developments in Artificial Intelligence Techniques for Prognostics – A Brief Survey	21
Pattern Recognition and Image Processing	25
Zalesky B. A., Lukashevich P. V. Scale Invariant Algorithm to Match Regions on Aero or Satellite Images	25
Therefore the state of the stat	31
Tableth recognition with roady ranges	35
bpocara inages	39
Zharkikh A. A., Bychkova S. M. Modeling of the Recognition Algorithm of Direction of Random Shift of Point on a Plane on a Random Rotations Background	43
	48
Gorshkova K., Shumsky I., Tsialiatnikau R. Photo Localization on Identification Documents in Conditions of Incomplete and Noisy Information	52
Algorithm of Pattern Recognition with Intra-Class Clustering	54
11	58
Vadapalli H. B., Nyongesa H., Omlin C. W. P. Classifying Facial Action Units: Use of Time Variant Data and Recurrent Neural Networks	64
reading of the object in colony of eparts	69
Grushetsky Y. E., Tuzikov A. V. Motions Space Clustering for Template-Based Protein Docking	73
Pradun D. V. Block-Parallel Clustering of Multispectral Images Using Max Flow Network Algorithm	76
Nedzved A., Nedzved O., Ablameyko S., Uchida S. Object Extraction at Nano-Surface Images	80
Naqvi S. A. Khattak T., Rehan W., Elahi A. A Novel Model for Face Recognition	84
Siddiqi M. H., Truc P. T. H., Lee S., Lee YK.	88
Farag A., Atta R., Mahdi H.	92

	Guzik P., Matiolański A., Orzechowski T. M., Dziech A. Evaluation of Parameters for Haar-Like Features Based Face Detection Algorithm 96
	Tulyakov S., Sadykhov R.
	Pace Recognition on Machine Readable Travel Documents: Algorithms and Results 99 Dvoenko S. D.
	On Clustering of a Set of Members by Distances and Similarities
	Khatami A., Mirghasemi S.
	A Hybrid Intelligent Algorithm-Based Color Space Conversion for Skin Detection 108
	Moreno R., Graña M., Ramik D. M., Madani K.
	Image Segmentation by Spherical Coordinates
	Fully-automated segmentation of tumor nuclei in cancer tissue images
	A Novel Technique of Partial Supervision for a Heuristic Algorithm of Possibilistic Clustering 121 Kharinov M.
	Adaptive Dichotomous Image Segmentation
	Sizov R., Kovalev T., Mironenko V., Prytkov V.
	Algorithms of Scarching and Marking Out Biological Objects
	Trekin A., Matveev I. A.
	Projection Method for Pupil Detection
	Knife Detection as a Subset of Object Detection Approach Based on Haar Cascades 139
	Ganchenko V., Petrovsky A., Pawlowski T.
	Special Areas Detection on Agricultural Fields Images Using Color Characteristics and Image Local Variability Evaluations
Da	ita Analysis 149
	Tarkov M. S., Tikhonov N. V.
	Evaluating the Thermogram Heterogeneity Based on Its Quadtree Representation 149
	Stankevich S. A., Starovoitov V. V., Shklyar S. V. Joint Subpixel Analysis of Different Spatial Resolution Multispectral and Hyperspectral
	Imagery
	Sergeeva K., Vorobejchikov S. An Efficient Algorithm for Detecting a Change Point of Autoregressive Parameters of AR(P)/ARCH(Q) Process
	Burkatovskaya Y., Vorobejchikov S.
	Sequential Procedure of Parameter Change Detection in AR/ARCH Process
	Dvoenko S. D., Panferov A. V. The Problem of Negative Eigenvalues Removing from Matrixes of Pairwise Comparisons . 165
	Kovalev V., Dmitruk A., Safonau I. A Method for Morphological Image Mining
	Marushko Y. Forecasting Multivariate Time Series Using Ensembles of Neural Network
	Podolskiy V. E.
	Simple Fuzzy Based Optimization Approach to the Problem of Dividing Outliers into Classes of Valuable and Noise Points
	Dotsenko A. S., Kondratenko Y. P. Computer Hand Gesture Recognition Using Fuzzy Logic
	Arroyo-Cañada FJ., Gil-Lafuente J.
	Effectiveness of Interactive Advertising Formats Versus Non Interactive in the Television Environment: a Simulation Based in Fuzzy Logic Analysis
	Viattchenin D. A.
	An Approach to Constructing a Possibility Distribution for the Number of Fuzzy Clusters 188 Liu R., Gillies D. F.
	Feature Selection Using Order Statistics

	Hancharou D., Nedzved A., Starovoitov V. V. Histological Image Stitching Algorithm Based on Normalized Statistical Moment 26	00
1.	Aliyeva N. T., Ismayilov E. A. Research of a Class of Smooth Membership Functions	04
	Butkin G., Zhuk D., Tuzikov A. V. Nonparametric Transforms for Describing Local Image Features	
	Chernov S., Kharin A. Error Probabilities Evaluation in Sequential Testing of Simple Hypotheses for Dependent Observations	13
	Muchen A. V. Chunuaev N. V. Shelyakov M. A.	16
	Cognitive Computer Technologies of Graphic Images Analysis	
Sig	nal Processing	19
	Piunovsky E. Using Wavelet Lifting Scheme for Audio Data Compression	219
	Aida-Zade K., Sharifova A.	
	Araa-Zaae K., Sharijota A. A comparison Between Allophone, Syllable, and Diphone Based TTS Systems for Azerbaijan Language	222
	Fedyayev O. I., Bondarenko I. Yu. Segment-Holistic Speech Recognition System Based on Model of Brain Hemispheric Interaction in Speech Perception	226
	Semenchik V., Pahomov V. Harmonic Signal Amplitude and Phase Measurement for Microwave Imaging System 2	231
	Bushra J., Fauvet E., Laligant O. Piecewise Image De-Noising Utilizing Discontinuous Edges	237
	Wassermann J., Dziech A. New Approach in Video Watermarking Based on DPCM and Transform Coding 2	241
	Stankevich A., Petrovsky Al., Petrovsky A. An FPGA-Based CABAC Module for Real-Time H.264/AVC Decoder	245
	Novikov A. E., Petrovsky A. Embedded DSP Module for Active Noise Control in Ventilation Systems	249
	Petrovsky N. A., Parfieniuk M. Distributed Arithmetic-Based Quaternion M-Band Wavelets Kernel for Multi-Resolution Analysis of Multimedia Data	253
	Kluchenya V. FPGA Architecture of DCT Processor Based on Lifting Steps for Real-Time Embedded	259
	Applications	
	Neural Network Model for Transient Ischemic Attacks Diagnostics	263
Sy	ystems and Parallel Architectures for Signal and Image 1 locusing	268
	Minkevičius S., Kulvietis G. A Mathematical Model of the Message Switching System	268
	Kulik B. Zuenko A., Fridman A.	271
	Archvodze N. Pkhovelishvili M., Shetsiruli L.	275
	Khanh N. Q. Security Requirements for SOA on the Base of Security Standards of Web-Service	280
	Mustafayev E. E., Hasanov J. Z., Sharifova A. The Device of Recognition and Scoring of Printed Texts	283
	Timchenko L., Kokriatskaia N., Melnikov V., Ivasyuk I., Makarenko R. Training the Parallel-Hierarchical Network for Recognition Static and Dynamic Images	286

Les H., Cellies D. F. Possinio Schillich Virilgi Ontol Schills on Research of the contract of

	Salnikov I. I. The Analysis of Distant Objects' Spatio-Temporal Parameters in Information Technical Systems	290
	Burmako E., Sadykhov R. Conflux: Embedding Massively Parallel Semantics in a High-Level Programming Language	
	Sadykhov R., Uvarov A., Pertsev D.	, 234
		299
Kn		303
	Artemieva I. L., Zuenko A., Fridman A. Integration of Ontologies, Knowledge and Data Archives into Ontology-Based Modeling Systems	303
	Gurevich I. Atoms, Molecules and Fundamental Restrictions on Characteristics of Information Systems	307
	Mamedova M. H., Djabrailova Z. G., Aliyev H. B. The method of Decision-Making Support for Employment of IT-Specialty Personnel Considering the Requirements of Employers	313
	Lbov G. S., Polyakova G. L. Forecasting Method Based on Logical Regularities	317
	Litvinskaya O. S., Salnikov I. I. Mathematical Decision Making Model for Selecting Implementation Means of Information Technical System	320
	Rusc T., Fornalski P., Dziech A., Slusarczyk P. Computer System for Management and Full-text Search of Court RecordsClasses	322
	Varlamov O. Mivar's Technologies to Development of Intelligent Systems and Project Development Active Multi-Subject Online Mivar's Encyclopedia	
	Djabrailova Z. G., Nobari S. M. Defining Methods of Importance Factor of the Criteria in the Solution of Personnel Management Problems and Detection of Contradictions	330
	Rustamov S. Structure and Contents of the Intellectual Systems, Which Ensure Human-Computer Dialogue	334
	Kaliukhovich D. Effect of Perceptual Expectancy on Neural Adaptation: Computational Approach	337
	Shut O. V. Logical and Precedent-related Approaches to Representation of Information in Pattern Recognition Problems: Comparative Analysis and Applications	339
	Krasnoproshin V., Obraztsov V., Vissia H. Knowledge Formalization in Decision Support Systems	
	Kostyukovich N. Yu., Shakah G., Valvachev A. N.	
	Modeling of Nature-Territorial Complexes Based on Organizational Structures	347
App	·	351
	Bogush R., Brovko N. An Efficient Smoke Detection Algorithm for Video Surveillance Systems Based on Optical Flow	351
	Megrelishvili R., Besiashvili G., Shengelia S. One-Way Cryptography Function Using $N \times N$ Matrices	
	Kumari L. L., Dharmaratne A. A Survey on Age Progression Techniques for Elderly People	358
,	Antidze J., Gulua N. Generalized Tools for Computer Realization of Natural Language Models	
	Ramík D. M., Sabourin Ch., Madani K. Hybrid Artificial Vision System Combining Salient Object Extraction and Machine-Learning	200

Myshev A. V. The Metrological Theory of Information Dynamics for Intelligent Tech-Nologies' Processes of Processing and Analyzing Information	370
Sergeev R. S., Tuzikov A. V., Eremin V. F. Statistical Approach to HIV-1 Mutation Analysis and Its Application	
Anfilets S. V., Kasyanik V. V., Shuts V. N. Application of Algorithms for Searching Motion in the Frame for the Detection of Vehicles 3	
Zaitseva E., Rusin M., Levashenko V. Reliability Analysis of Complex System	381
Pisarenko V., Pisarenko J. Some Algorithms of UAV's Coordinates Definition by Onboard Processor According to Videocameras	387
Kabysh A., Golovko V., Mikhniayeu A., Rubanau U., Lipnikas A. Behavior Patterns of Adaptive Multi-Joined Robot Learned by Multi-Agent Influence Reinforcement Learning	
Vaitsekhovich L., Golovko V., Madani K. Modeling of Multi-Agent Intrusion Detection System Based on Interaction Graph of Agents 3	397
Diomin V., Kostiuk D., Nikoniuk A. Dynamic Windows Scaling in Unix-Like Systems Interface	
Baranauskas V., Bartkevičius S., Šarkauskas K., Kabysh A. Using Vector Marks for Robot Navigation	406
Krasnoproshin V., Mazouka D. Graphics Pipeline Automation Based on Visualization Algebra	410
Liu H., Krasnoproshin V. Electronic Commerce Websites Evaluation Based on Fuzzy Analytic Hierarchy Process 4	413
Avakaw S., Doudkin A., Voronov A., Orlova T. Software Applications of Input Data Preparation for Single-Beam Layout Generator of IC Topology	417
Inyutin A. Algorithm of the PCB Topology Inspection and Defects Classification	422
Kuzmich A. I., Shakah G., Valvachev A. N. Remote Monitoring System for Mobile Objects	427
Avakaw S. M., Doudkin A., Inyutin A., Rusetsky S. A., Otwagin A. V. Paralleling Aerial Image Simulation Based Multi-Agent Approach for Photolithography . 4	431
Podenok L. P., On Modular Exponentiation in Residue Number System	
Image Processing and Modeling Struts S. V., Matveev I. A.	442
Reconstruction of 3D Structure of Human Face Using a Pair of Images and 3D Model of Human Face	442
Podkosova Y., Vasiuhova S. A., Varlamov O. Use of Technologies of the Virtual Reality in Three-Dimensional Visualization of Results and Mivar's Application of Training Systems	447
Amarger V., Ramík D. M., Moreno R., Rossi L., Madani K., Graña M. Wildland Fires' Outlines Extraction: a Spherical Coordinates Framed RGB Color Space Dichromatic Reflection Model Based Image Segmentation	451
Losik G. A Recognition Model Using Objects Variability Information	455
Kapura V., Sachenko A., Roth H., Adamiv O. Method of Stereoimage Fusion for 3D Reconstruction	461
bject Index	46 4
thor Index	468

Histological Image Stitching Algorithm Based on Normalized Statistical Moment

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Abstract: The problem considered in this paper is the automatic histological image stitching. In this paper, invariant local features based on normalized statistical moment are used to select matching points and calculate the translation. This algorithm consists of feature detection, feature registration and spatial transition. The experimental results with histological images in different categories demonstrate this algorithm is fast, effective and does not require human interaction.

Keywords: Image Stitching, Harris Detector, Normalized Statistical Moment (NSM)

1. INTRODUCTION

Stitching techniques have been used to combine overlapped signals into a new one with as little distortion of each signal as possible. Building a stitched image from a sequence of partial views is a powerful means of obtaining a complete, non-redundant view of scene [1]. Image stitching has been applied in medicine, computer vision and photogrammetry.

In general, most image stitching techniques developed in recent years can be divided into two categories: template and feature based. Template based algorithms attempt to correlate the grey levels of image patches in the views, assuming that they present some similarity [2]. Feature based algorithms establish correspondences between points, lines or other geometrical entities and use properties of local intensity values to match them.

In our application, overlapping images are used to construct an image with a far larger field of view. It solves the problem that histological image covers a very small area. The approach proposed in this paper as shown in Fig.1 extracts interesting points by Harris corner detector and then matches them using a NSM technique followed by a statistical procedure. We choose Harris corner detector here due to its invariant to geometric transformations. NSM feature which belongs to invariant image feature is from physical conceptions. Experimental results show that the NSM feature of image has the ability of antitonal and geometric distortion (translation, rotation and scaling, TRS) and its extracting method is simple [3]. Thus, NSM feature offers a solution to correlate interesting points and recover the translation between images.

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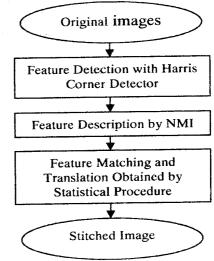


Fig. 1. The pipeline of image stitching

2. FEATURE DETECTION

The Harris measure M is the second moment matrix, describing the curvature of the autocorrelation function in the neighborhood of a point [4].

$$M = w_{u,v} * \begin{pmatrix} L_x^2 & L_x L_y \\ L_y L_x & L_y^2 \end{pmatrix}.$$
 (1)

where * is convolution operator and $w_{u,v} = e^{\frac{-(u^2+v^2)}{2\sigma^2}}$ a Gaussian smoothing window. We can get image L_x from image I_x smoothed by a Gaussian $L_x^2 = I_x^2 * w_{u,v}$.

And the first gradients I_x and I_y in x, y direction respectively are approximated by

$$I_{x} = I * (-1,0,1) \approx \partial I / \partial x.$$
 (2)

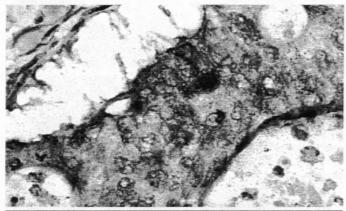
$$I_{\cdot,\cdot} = I * (-1,0,1)^T \approx \partial I / \partial y . \tag{3}$$

Let α , β be eigenvalues of M. α and β will be proportional to the principal curvatures of local autocorrelation function and form a rotationally invariant description of M [5, 6]. A corner point will have an M with two strong eigenvalues. An edge will present one strong and one weak eigenvalue and a flat region will have two weak eigenvalues.

Now, we can measure the corner response R with eigenvalues α and β , thus

$$R = Det(M) - kTr^{2}(M). (4)$$

Where $Det(M) = \alpha * \beta$, $Tr(M) = \alpha + \beta$. R is positive in the corner region, negative in the edge region, and small in the flat region [5]. An interesting point is selected as a corner pixel by applying high threshold as shown in Fig.2.



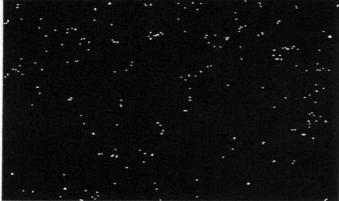


Fig. 2. Histological image with interesting points in blue with the threshold 5000

3. FEATURE DESCRIPTION

The definition of NSM is as follows:

$$NMI = \frac{\sqrt{J_{(cx,cy)}}}{\sum_{y=1}^{M} \sum_{y=1}^{N} f(x,y)}.$$
 (5)

where (cx, cy) is the center of mass of the image and $J_{(cx,cy)}$ the statistical moment.

$$cx = \frac{\sum_{x=1}^{M} \sum_{y=1}^{N} x \times f(x, y)}{\sum_{x=1}^{M} \sum_{y=1}^{N} f(x, y)}.$$
 (6)

$$cy = \frac{\sum_{x=1}^{M} \sum_{y=1}^{N} y \times f(x, y)}{\sum_{x=1}^{M} \sum_{y=1}^{N} y}$$
(7)

$$J_{(cx,cy)} = \sum_{v=1}^{M} \sum_{v=1}^{N} ((x - cx)^2 + (y - cy)^2) f(x,y).$$
 (8)

NSM feature is invariant to translation, rotation and scaling. In our application, we use NSM to describe the interesting points in images. The approach calculates NSM for a disk around the points and the same points in different images will have similar properties.

4. FEATURE MATCHING

In our application we only consider translation between images though tiny rotation and scaling may exist from measure errors. Feature matching is performed with NSM and centers of gravity corresponding to interesting points between images. We define a measure of the strength of the match (SM for abbreviation), as

$$SM(NMI_{1i}, NMI_{2j}) = \frac{\left|NMI_{1i} - NMI_{2j}\right|}{0.5 * (NMI_{1i} - NMI_{2j})}.$$
 (9)

 NMI_{1i} is the NSM of i-th interesting point in the first image and NMI_{2j} the j-th in the second image. Let $G_{1i}(x,y)$ and $G_{2j}(x,y)$ are the centers of gravity.

If $SM(NMI_{1i}, NMI_{2j}) \le 0.1$ and $Dist(G_{1i}, G_{2j}) \le 0.1$, then the pair of interesting points is a potential match. $Dist(G_{1i}, G_{2j})$ is defined as follows.

$$Dist(G_{1i}, G_{2j}) = \sqrt{(x_{1i} - x_{2j})^2 + (y_{1i} - y_{2j})^2} . \tag{10}$$

Until now the match relationship is multi-to-multi and the purpose is to contain correct matches in potential matches. For every pair of math points, calculate translation in x and y directions each, then we can get a statistical char of quantities of matching points at different translation as shown if Fig.4. Correct matching points will result in same translation and others are stochastic, so maximum exists at proper translation between images in theory. In practice, we use following expression to estimate.

$$score = \frac{Num_x(best)}{Num_x(\sec ond)} + \frac{Num_y(best)}{Num_y(\sec ond)}.$$
 (11)

 $Num_x(best)$ and $Num_x(second)$ mean the number of best and second best match in x direction in the statistical chart. If the condition score > 1.2 is met, these two images are treated as overlapped and the location of maximum in the chart is the translation between them.

5 EXPRERIMENTAL RESULTS

The proposed algorithm has been evaluated by histological images and pathological images and good stitching results have been obtained.

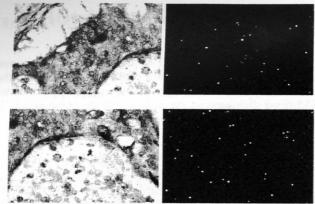


Fig.3. Two partially overlapped histological images (top) and the images with detected interesting points (bottom)

Fig.3 shows two original overlapped histological marrow images and interesting points which are detected by Harris corner detector with the threshold 5000. For such a color image, we only use intensity component to calculate interesting points and NSM.

After feature matching, the statistical cart of distance of matching points is shown in Fig.4. We can easily find maximums in each direction and this can demonstrate the robustness of our algorithm. The location of peak value on x and y axis is the translation between the two images to be stitched and in this case the peak is at (313, 50). The stitching result is shown in Fig.5.

This method can achieve fast image stitching and the time elapsed during the procedure of feature detection and feature matching is theoretical proportional to the number of interesting points. Table 1 compares the time consumed of NSM based method with Zernike moment [4], phase correlation [6] methods in image stitching and the results are average time of experiments on same size images. Fig.6 shows the mosaic results based on these two methods.

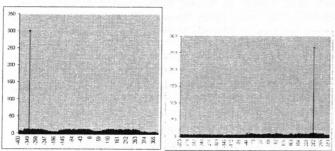


Fig.4. The statistical chart of quantities of matching points at different translation in x direction (left) and y direction (right)

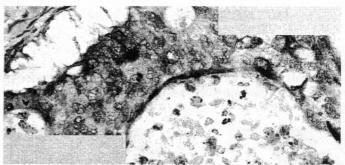


Fig.5. Stitching image by the translation obtained in Fig.4

NSM based mosaic result shown in Fig.5 is almost the same as Zernike moment and phase correlation based results shown in Fig.6, but their efficiency is distinct. Table 1 demonstrates that NSM based method is much faster in stitching images with translation. Its advantage becomes more prominent when the size of images increases. Fig.7 shows image stitching with NSM.

Table 1. A comparison of time-consuming of three different methods (unit: ms)

Image size	NSM	Zernike Moment	Phase Correlation
1798x1438	5601	47631	44692
2592x1944	9659	65798	174676

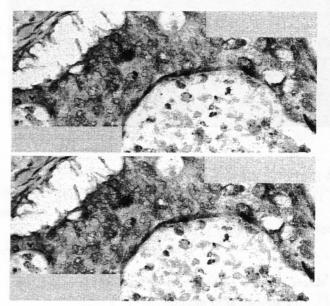


Fig.6. Mosaic based on Zernike moment (top) and phase correlation (bottom)

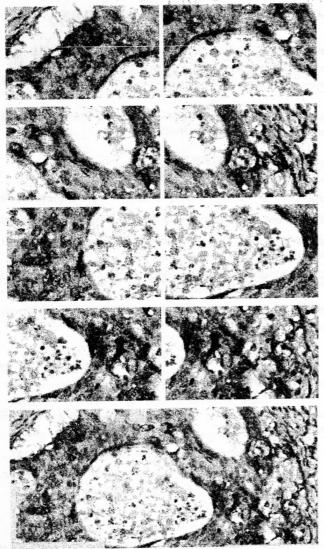


Fig.7. Original partially overlapped images to be stitched (top) and the stitching result with NSM (bottom)

6. CONCLUSION

In this paper, a novel approach based on normalized statistical moment to solve the histological image stitching problem has been proposed. The algorithm can calculate and recover the translation between the images quickly and efficiently to completely meet the demands of stitching histological medical images. Our experiments with histological images in different categories have demonstrated the proposed algorithm's robustness and speed, so it has been successfully integrated in our automatic histological image analysis system.

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